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(54) Title: BIODEGRADABLE SUSTAINED-RELEASE ALGINATE GELS			
(57) Abstract The present invention relates to sustained-release formulations using biodegradable alginate delayed gels or particles and methods thereof.			

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BIODEGRADABLE SUSTAINED-RELEASE ALGINATE GELS

FIELD OF THE INVENTION

5 The present invention relates to sustained-release formulations using biodegradable alginate gel beads and/or delayed gels and methods thereof.

BACKGROUND OF THE INVENTION

10 With the advances in genetic and cell engineering technologies, the availability of recombinant proteins has engendered advances in the use of proteins as medicaments for therapeutic
15 applications. Many illnesses or conditions treated with pharmaceutical proteins require sustained protein levels to achieve the most effective therapeutic result. However, as with most protein pharmaceuticals, the generally short biological half-life requires
20 frequent administration. These repeated injections are given at various intervals which result in fluctuating medication levels at a significant physical and monetary burden on the patients. Since many conditions respond better to controlled levels of a
25 pharmaceutical, a need exists for controlled release of a medicament to provide longer periods of consistent release. Such sustained-release medicaments would provide the patient with not only enhanced prophylactic, therapeutic or diagnostic effects, but
30 also a decrease in the frequency of injections as well as in overall costs.

 Current attempts to sustain medication levels in humans or animals between doses have included the use of biodegradable polymers as matrices to control
35 medicament release. For example, Great Britain Patent No. 1,388,580 discloses the use of hydrogels for

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sustained-release of insulin. U.S. Patent No. 4,789,550 discloses the use of polylysine coated alginate microcapsules for delivery of protein by encapsulating living cells. Sustained-release attempts
5 have also utilized anionic or cationic polymer compositions surrounded by ionic polymers of the opposite charge for encapsulating cells capable of producing biologically active compositions; U.S. Patent No. 4,744,933. Likewise, multiple coats of anionic or
10 cationic cross-linking polymers have also been disclosed as means for obtaining controlled release; U.S. Patent Nos. 4,690,682 and 4,789,516. In addition, further attempts disclose the use of alginates alone, or alginates coated with other biodegradable polymers,
15 for controlled release of polypeptide compositions or cation precipitates thereof; PCT WO 96/00081, PCT WO 95/29664 and PCT WO 96/03116.

These attempts, however, have provided insufficient means for obtaining sustained-release
20 delivery of desired protein pharmaceuticals. It is generally known that the use of certain biodegradable polymers, e.g., polylactide co-glycolide, under *in vivo* conditions, exhibit high initial bursts of medicament release; Johnson, O. et al., Nature Med., 2(7): 795
25 (1996). Furthermore, it is generally known that proteins used with current forms of sustained-release preparations can undergo denaturation and lose their bioactivity upon exposure to the encapsulating agents. Such preparations use organic solvents which can have
30 deleterious effects on the protein of choice. Finally, as discussed below, use of alginate alone has not provided the desired controlled protein release necessary for effective therapeutic results.

In general, alginates are well known,
35 naturally occurring, anionic, polysaccharides comprised of 1,4-linked- β -D-mannuronic acid and α -L-guluronic

acid; Smidsrod, O. et al., Trends in Biotechnol., 8: 71-78 (1990); Aslani, P. et al., J. Microencapsulation, 13(5): 601-614 (1996). Alginates typically vary from 70% mannuronic acid and 30% guluronic acid, to 5 30% mannuronic acid and 70% guluronic acid; Smidsrod, supra. Alginic acid is water insoluble whereas salts formed with monovalent ions like sodium, potassium and ammonium are water soluble; McDowell, R.H., "Properties of Alginates" (London, Alginate Industries Ltd, 4th 10 edition 1977). Polyvalent cations are known to react with alginates and to spontaneously form gels.

Alginates have a wide variety of applications such as food additives, adhesives, pharmaceutical tablets and wound dressings. Alginates have also been 15 recommended for protein separation techniques. For example, Gray, C.J. et al., in Biotechnology and Bioengineering, 31: 607-612 (1988) entrapped insulin in zinc/calcium alginate gels for separation of insulin from other serum proteins.

20 Alginate matrices have also been well documented for drug delivery systems; see for example, U.S. Patent No. 4,695,463 which discloses an alginate based chewing gum delivery system and pharmaceutical preparations. Alginate beads have been used for 25 controlled release of various proteins such as: tumor necrosis factor receptor in cation-alginate beads coated with polycations; Wee, S.F, Proceed. Intern. Symp. Control. Rel. Bioact. Mater., 21: 730-31 (1994); transforming growth factor encapsulated in alginate 30 beads; Puolakkainen, P.A. et al., Gastroenterology, 107: 1319-1326 (1994); angiogenic factors entrapped in calcium-alginate beads; Downs, E.C. et al., J. of Cellular Physiology, 152: 422-429 (1992); albumin entrapped in chitosan-alginate microcapsules; Polk, A. 35 et al., J. Pharmaceutical Sciences, 83(2): 178-185 (1994); chitosan-calcium alginate beads coated with

polymers; Okhamafe, A. O. *et al.*, J. Microencapsul., 13(5): 497-508 (1996); hemoglobin encapsulated with chitosan-calcium alginate beads; Huguet, M.L. *et al.*, J. Applied Polymer Science, 51: 1427-1432 (1994),
5 Huguet, M.L. *et al.*, Process Biochemistry, 31: 745-751 (1996); and interleukin-2 encapsulated in alginate-chitosan microspheres; Liu, L.S. *et al.*, Proceed. Intern. Symp. Control. Rel. Bioact. Mater, 22: 542-543 (1995).

10 Systems using alginate gel beads, or alginate/calcium gel beads, to entrap proteins suffer from lack of any sustained-release effect due to rapid release of the protein from the alginate beads; Liu, L. *et al.*, J. Control. Rel., 43: 65-74 (1997). To avoid
15 such rapid release, a number of the above systems attempt to use polycation polymer coatings (e.g., polylysine, chitosan) to retard the release of the protein alginate beads; *See*, e.g., Wheatley, M.A. *et al.*, J. Applied Polymer Science, 43: 2123-2135 (1991);
20 Wee, S.F. *et al.* *supra*; Liu, L.S. *et al.* *supra*; Wee, S.F. *et al.*, Controlled Release Society, 22: 566-567 (1995) and Lim, *et al.* *supra*.

Polycations, such as polylysine, are positively charged polyelectrolytes which interact with
25 the negatively charged alginate molecules to form a polyelectrolyte complexes that act as diffusion barriers on the bead surface. Problems can occur with the use of polycations in that: (1) such formulations maybe cytotoxic due to the polycations; Huguet, M.L. *et al.*, *supra*; Zimmermann, Ulrich, Electrophoresis, 13: 269 (1992); Bergmann, P. *et al.*, Clinial Science, 67: 35 (1984); (2) polycations are prone to oxidation; (3) beads with polycation coatings tend not to be erodible and build up in the body; (4) such
35 formulations are made via laborious coating procedures which include multiple coatings of the polycation

polylysine; Padol, *et al.*, *Proceed. Intern. Symp. Control. Rel. Bioact. Mater.*, 2: 216 (1986) and (5) ionic interactions between the protein and the polycations can result in loss of protein activity or
5 cause protein instability.

Francesco *et al.*, U.S. Patent No. 5,336,668 (and references cited therein) describe total and partial esters of alginic acid, made by different processes, and possessing interesting pharmaceutical
10 qualities. It is described how the alginic esters could be utilized as biodegradable plastic materials for medical-surgical use; as additives for a wide range of polymeric materials; or used in the preparation of various medicaments. Potential use the esterified
15 alginates in sustained release formulations is not discussed nor are esterified alginate hydrogels described.

Nightlinger *et al.*, *Proceed. Inter. Symp. Control. Rel. Bioact. Mater.*, 22: 738-739 (1995)
20 describe esterified hyaluronic acid (HA) microspheres having controlled release capabilities. The references generally addresses the different degradation rates for their HA derivatives and describe how the ester "breaks off" to liberate the alcohol and HA moieties. There is
25 no discussion relating how or whether the HA backbone itself breaks down into lower molecular weight polymer units.

In order for a polysaccharide based sustained delivery system to be useful, the polysaccharide must
30 be biodegradable into non-toxic products. It has been found that certain alginate gel systems, while effective in providing sustained release of drug, results in a "bump" (or nodule) at the site of injection due to the very slow dissipation of the gel.
35 In a therapeutic setting involving low doses of drug and infrequent injections, this might not be a major

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problem. However, in a therapeutic setting involving high doses of drug and more frequent injections, this effect could be prohibitive. A means for increasing the dissipation rate of the alginate gel from the injection site must be developed.

There is thus still a need to develop pharmaceutical formulations which achieve a more versatile and effective means of sustained-release for clinical applications. Numerous recombinant or natural proteins could benefit from constant long term release and thereby provide more effective clinical results.

The present invention provides such advances. Pharmaceutical compositions using the biodegradable alginate gel particles or gels of the present invention are capable of providing increased bioavailability, protein protection, decreased degradation and slow release with increased protein stability and potency. Also, pharmaceutical compositions of the present invention provide a simple, rapid and inexpensive means of controlled recombinant protein release for effective prophylactic, therapeutic or diagnostic results.

SUMMARY OF THE INVENTION

The present invention grew out of studies using unmodified alginate (a class of anionic polysaccharides) hydrogels for the sustained release of proteins. These protein-containing unmodified alginate hydrogels (see copending U.S. applications 08/857,913 and 08/912,902) are formed in a time-delayed manner whereby the materials can be filled in a syringe and left to later gel in the same syringe; these gels are found to be injectable. After a single subcutaneous injection in rodent models evidence of many days of sustained protein is observed; however, a perceptible bump or nodule remains at the injection site for long

periods of time with little change in its size. This bump consists of the water-filled alginate hydrogel and the size of the bump is a function of the volume of gel that is injected. Gel beads also remain at the
5 injection site.

The present invention thus relates to a novel class of biodegradable biocompatible polysaccharide hydrogels, e.g., alginate ester hydrogels, for the sustained release of therapeutic proteins.
10 Unexpectedly, the alginate ester hydrogels, in addition to having the gelation, injectability and sustained release properties of the unmodified alginates, did not leave a bump at the injection site---that is, the alginate ester hydrogels are biodegradable or erodible
15 and are gradually resorbed into the surrounding tissues with little injection site reaction.

The compositions of the present invention comprise alginate esters or their derivatives ionically crosslinked in a hydrogel (water-containing) matrix
20 containing a therapeutic agent such as a protein.

The present invention further relates to a method of producing biodegradable sustained release compositions.

The present invention further relates to the
25 use of the ester alginate materials in liquid mixtures for time delay gelation in the body.

The present invention further relates to compositions wherein the alginate ester hydrogels are in the form of beads or microspheres for the sustained
30 release of active agents preferably therapeutic proteins.

In one embodiment of the present invention the alginate ester hydrogels provide compositions for application at target sites in the body of a patient.
35 These compositions are useful: for preventing or inhibiting the formation of tissue adhesions following

surgery and traumatic injury; for supplementing tissues especially for filling soft and hard tissues; to fill a confined space with a resorbable material; as a scaffold for tissue growth; and as a wound dressing.

5 In another embodiment the alginate ester hydrogels provide active agent containing devices for implantation in the body whereby the agent can be either bound or unbound to the alginate polymer.

In another embodiment the alginate ester
10 hydrogel compositions of the present invention provide a method for improving the bioavailability of the active agent in the composition.

Finally, the alginate ester hydrogel
compositions of the present invention further provide a
15 method for obtaining a substantially constant blood level over time in the patient.

DETAILED DESCRIPTION OF THE INVENTION

20 Compositions

Hydrophilic polymers including alginates and derivatives thereof, can be obtained from various commercial, natural or synthetic sources well known in the art. As used herein, the term hydrophilic polymer
25 refers to water soluble polymers or polymers having affinity for absorbing water. Hydrophilic polymers are well known to one skilled in the art. These include but are not limited to polyanions, including anionic polysaccharides such as alginate, carboxymethyl
30 amylose, polyacrylic acid salts, polymethacrylic acid salts, ethylene maleic anhydride copolymer (half ester), carboxymethyl cellulose, dextran sulfate, heparin, carboxymethyl dextran, carboxy cellulose, 2,3-dicarboxycellulose, tricarboxycellulose, carboxy
35 gum arabic, carboxy carrageenan, pectin, carboxy pectin, carboxy tragacanth gum, carboxy xanthan gum,

pentosan polysulfate, carboxy starch, carboxymethyl
chitin/chitosan, curdlan, inositol hexasulfate,
b-cyclodextrin sulfate, hyaluronic acid,
chondroitin-6-sulfate, dermatan sulfate, heparin
5 sulfate, carboxymethyl starch, carrageenan,
polygalacturonate, carboxy guar gum, polyphosphate,
polyaldehyde-carbonic acid, poly-1-hydroxy-1-sulfonate-
propen-2, copolystyrene maleic acid, agarose,
mesoglycan, sulfopropylated polyvinyl alcohols,
10 cellulose sulfate, protamine sulfate, phospho guar gum,
polyglutamic acid, polyaspartic acid, polyamino acids,
derivatives or combinations thereof. One skilled in
the art will appreciate other various hydrophilic
polymers that are within the scope of the present
15 invention.

Likewise, bound polyvalent metal ions can be
obtained from various commercial, natural or synthetic
sources which are well known in the art. In
particular, the metal ions can include but are not
20 limited to aluminum, barium, calcium, iron, manganese
magnesium, strontium and zinc. Preferably the metal
ions are calcium and zinc or the salts thereof, like
zinc acetate, calcium acetate or chloride salts. Water
soluble small molecules and salts can also be used such
25 as ammonium sulfate, acetone, ethanol and glycerol.

Alcohols of the aliphatic series for use as
esterifying components of the carboxy groups of alginic
acid according to the present invention are, for
example, those with a maximum of 34 carbon atoms, which
30 may be saturated or unsaturated and which may possibly
also be substituted by other free or functionally
modified groups, such as amino, hydroxy, aldehyde,
keto, mercapto, carboxy groups or by groups deriving
from the same, such as hydrocarbyl or
35 dihydrocarbylamino (hereafter the term "hydrocarbyl"

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should be taken to mean not only monovalent radicals of hydrocarbons such as the C_nH_{2n+1} type but also

bivalent or trivalent radicals, such as

"alkylenes"- C_nH_2 , or "alkylidenes" (= C_nH_{2n}), ether or

- 5 ester groups, acetal or ketal groups, thio-ether or thioester groups and esterified carboxy groups or carbamidic or carbamidic groups substituted by one or two hydroxy groups, by nitrile groups or by halogens.

- In the above groups containing hydrocarbyl
10 radicals these are preferably lower aliphatic radicals, such as heteroatoms, such as oxygen, nitrogen and sulfur. Preference is given to alcohols substituted with one or two of the aforesaid function groups.

- Alcohols of the above group to be used
15 preferentially within the terms of the present invention are those with a maximum of 12 and especially with a maximum of 6 carbon atoms and in which the hydrocarbyl radicals in the above mentioned amino, ether, ester, thioether, thioester, acetal,
20 ketal groups representing alkyl groups with a maximum of 4 carbon atoms, and also in the esterified carboxy or substituted carbamidic groups the hydrocarbyl groups are alkyls with the same number of carbon atoms, and in which the amino or carbamidic groups may be
25 alkyleneamino or alkylene carbamidic groups with a maximum of 8 carbon atoms. Of these alcohols those to be mentioned first and foremost are the saturated and unsubstituted ones such as methyl, ethyl, propyl, isopropyl alcohols, n-butyl alcohol, isobutyl, tert-
30 butyl alcohols, amyl, pentyl, hexyl, octyl, nonyl, and dodecyl alcohols and above all those with a linear chain such as n-octyl or n-dodecyl alcohols. Of the substituted alcohols of this group the bivalent alcohols should be listed, such as ethyleneglycol,
35 propylene glycol or butylene glycol, the trivalent alcohols such as glycerin, aldehyde alcohols such as

tartronic alcohol, carboxy alcohols such as lactic acids, for example alpha-oxypropionic acid, glycolic acid, malic acid, tartaric acids, citric acid, aminoalcohols, such as aminoethanol, aminopropanol, 5 n-aminobutanol and their dimethyl and diethyl derivatives in the aminic function, choline, pyrrolidinyethanol, piperidinyethanol, piperazinylethanol and the corresponding derivatives of n-propyl or n-butyl alcohols, monothioethyleneglycol or 10 its alkyl derivatives, for example the ethyl derivative in the mercapto function.

Of the higher saturated aliphatic alcohols, those worthy of special mention are for example cetyl alcohol and myristyl alcohol, but especially important 15 for the purposes of the present invention are the higher unsaturated alcohols with one or two double bonds, such as especially those contained in many essential oils and having an affinity with terpenes such as citronellol, geraniol, nerol, nerolidol, 20 linalool, farnesol, phytol.

Of the lower unsaturated alcohols consideration should be given to propargyl alcohol.

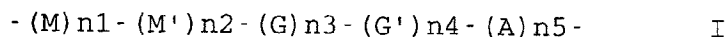
Of the aliphatic alcohols those to be 25 mentioned above all are those with only one benzene residue and in which the aliphatic chain has a maximum of 4 carbon atoms, in which also the benzene residue may be substituted by between 1 and 3 methyl or hydroxy groups or by halogen atoms, especially chlorine, 30 bromine or iodine and in which the aliphatic chain may be substituted by one or more functional groups selected from the group consisting of free amino groups or mono- or dimethyl groups or by pyrrolidine or piperidine groups. Of these alcohols, benzyl alcohol 35 and phenethyl alcohol are especially preferred. The alcohols of the cycloaliphatic or aliphatic

cycloaliphatic series may derive from mono or polycyclic hydrocarbons and may have a maximum of 34 carbon atoms. Of the alcohols derived from cyclic monoanular hydrocarbons special mention should be given to those with a maximum of 12 carbon atoms, with rings containing preferably between 5 and 7 carbon atoms, possibly substituted for example by between one and three lower alkyl groups, such as methyl, ethyl, propyl or isopropyl groups. Specific alcohols of this group are cyclohexanol, cyclohexanediol, 1,2,3-cyclohexanetriol and 1,3,5-cyclohexanetriol (phloroglucitol), inositol, the alcohols deriving from p-menthane such as carvomenthol menthol, alpha and gamma-terpineol 1-terpineol alcohols known as "terpineol", 1,4-and 1,8-terpin. Alcohols deriving from hydrocarbons with condensed rings are, for example, those of the thujane, pinane, camphane groups, particularly thujanol, sabinol pinol hydrate, D and L-borneol and D and L-isoborneol.

Also to be included are alcohols derived from the esterification reaction of epoxy-containing compounds with alginates (See e.g., U.S. Patent 2,463,824 and U.S. Patent 2,426,125).

The total and partial ester group containing polyanions of the present invention are generally acidic polysaccharides where the glycosidic oxygen is attached beta to the carbonyl carbon of the ester. While not being bound to any specific mechanism, this arrangement of the moieties allows the breakdown of the polymer chain by a beta-elimination mechanism which can occur under physiological conditions.

Alginic acid esters of the present invention are comprised of mannuronic acid residues (m-COOH or m-COO anion) and guluronic acid residues (g-COOH or g-COO anion) joined together by glycosidic ether oxygen linkages of the following general formula I:



where:

- 5 M is a mannuronic acid residue, m-COOH or m-COO anion;
 M' is a mannuronic acid ester residue, m-COOR₁;
 G is a guluronic acid residue, g-COOH or g-COO anion;
 G' is a guluronic acid ester residue, g-COOR₂;
 A represents non-g or non-m chain units, such as
 10 sugars, sugar oxidation products, or aliphatic,
 aromatic, araliphatic, alaromatic, cycloaliphatic
 radicals which can be substituted and interrupted by
 heteroatoms linked within or at the chain ends;
 n₁, n₂, n₃, n₄ and n₅ are integers representing the
 15 average relative number of incorporated units;
 R₁ and R₂ are independently aliphatic, aromatic,
 araliphatic, alaromatic, cycloaliphatic radicals which
 can be substituted and interrupted by heteroatoms;
 and derivatives (e.g. where the hydroxy groups are
 20 acetylated and are reacted with isocyanates) and
 pharmaceutically acceptable salts thereof.

In the esters of the present invention, it is
 desirable that R₁ = R₂ = aliphatic or alaromatic and
 further that $100(n_2+n_4)/(n_1+n_2+n_3+n_4)$ is from 1-99
 25 mol%, preferably 5-50 mol%, more preferably 6-30 mol%,
 still more preferably 6-15 mol% and most preferably
 7-12 mol% and $100n_5/(n_1+n_2+n_3+n_4+n_5)$ is preferably less
 than 10 mol%.

In the partial esters of the invention the
 30 non-esterified carboxy groups may be kept free or may
 be salified. The bases for the formation of these
 salts are chosen according to the ultimate end use of
 the product. Inorganic salts may be formed from
 alkaline metals, such as potassium and in particular
 35 sodium and ammonium, or deriving from alkaline earth
 metals such as calcium or magnesium or aluminum salts.

Of particular interest are the salts with organic bases, especially azotized bases and, therefore, aliphatic, araliphatic, cycloaliphatic or heterocyclic amines. These ammonium salts may derive
5 from therapeutically acceptable amines or nontoxic but therapeutically inactive amines, or from amines with a therapeutic action. Of the first type, preferred are aliphatic amines, for example mono-, di- and tri-alkylamines with alkyl groups with a maximum of 8
10 carbon atoms or arylalkylamines with the same number of carbon atoms in the aliphatic part and where aryl means a benzene group possibly substituted by between 1 and 3 methyl groups or halogen atoms or hydroxy groups. The biologically inactive bases for the formation of the
15 salts may also be cyclic, such as monocyclic alkyleneamines with cycles of between 4 and 6 carbon atoms, possibly interrupted in their cycle by heteroatoms chosen from the group formed by nitrogen, oxygen and sulphur, such as piperazine or morpholine,
20 or may be substituted, for example by amino or hydroxy functions such as aminoethanol, ethylenediamol, ethylenediamine, ephedrine or choline.

The degree of and type of esterification can be controlled by synthetic methods known in the art.
25 Preferably, the alginate esters are prepared by treatment of the quaternary ammonium salts of alginic acid with conventional alkylating agents in an aprotic organic solvent such as dimethyl sulfoxide. The resultant esters are preferably the esters of
30 monovalent alcohols such as lower alkyl such as ethyl or aralkyl such as benzyl or their mixtures. One can also form esters by the reaction of alginic acid with oxirane or epoxy containing compounds such as ethylene or propylene oxide.

35 It is also possible to form quaternary ammonium salts of partial esters, for example the salts

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of tetraalkylammonium with the above said number of carbonatoms and-preferably salts of this type in which the fourth alkyl group has between 1 and 4 carbon atoms, for example a methyl group.

5 The degree of esterification (expressed in mol%) of the alginate is related to the desired disappearance rate of the gel in the patient tissue. This disappearance rate of the gel is generally related to the desired release rate of the active agent from
10 the gel that is over a period of 5 years or less, usually 2 days to 270 days, more usually 2 days to 180 days, more usually 2 days to 90 days. The degree of esterification (DE) is from 1 mol% to 99 mol%, preferably from 5 mol% to 50 mol%, more preferably from
15 6 mol% to 30 mol%, more preferably from 6 mol% to 15 mol%, more preferably from 7 mol% to 12 mol%.

As used herein, the term buffer or buffer solution refers to use of inorganic or organic acids or a combination thereof to prepare a buffer solution as
20 known in the art. Inorganic acids within the scope of the present invention include hydrogen halide (e.g., hydrochloric acid), phosphoric, nitric or sulfuric. Other inorganic acids would be well known to one skilled in the art and are contemplated herein. Organic
25 acids within the scope of the invention include aliphatic carboxylic acids and aromatic acids such as formic, carbonic, acetic, propionic, butyric, valeric, caproic, acrylic, malonic, succinic, glutaric, adipic, maleic, fumaric, glycine or phenol sulfonic. Other
30 organic acids would be well known to one skilled in the art.

As used herein, biologically active agents refers to recombinant or naturally occurring proteins, whether human or animal, useful for prophylactic,
35 therapeutic or diagnostic application, as well as non-protein based agents such as small molecules. The

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biologically active agent can be natural, synthetic, semi-synthetic or derivatives thereof. The biologically active agents of the present invention must be precipitable. A wide range of biologically active agents are contemplated. These include but are not limited to hormones, cytokines, hematopoietic factors, growth factors, antiobesity factors, trophic factors, anti-inflammatory factors, and enzymes (see also U.S. Patent No. 4,695,463 for additional examples of useful biologically active agents). One skilled in the art will readily be able to adapt a desired biologically active agent to the compositions of present invention.

Such proteins would include but are not limited to interferons (see, U.S. Patent Nos. 5,372,808, 5,541,293 4,897,471, and 4,695,623 hereby incorporated by reference including drawings), interleukins (see, U.S. Patent No. 5,075,222, hereby incorporated by reference including drawings), erythropoietins (see, U.S. Patent Nos. 4,703,008, 5,441,868, 5,618,698 5,547,933, and 5,621,080 hereby incorporated by reference including drawings), granulocyte-colony stimulating factors (see, U.S. Patent Nos. 4,810,643, 4,999,291, 5,581,476, 5,582,823, and PCT Publication No. 94/17185, hereby incorporated by reference including drawings), stem cell factor (PCT Publication Nos. 91/05795, 92/17505 and 95/17206, hereby incorporated by reference including drawings), and the OB protein (see PCT publication Nos. 96/40912, 96/05309, 97/00128, 97/01010 and 97/06816 hereby incorporated by reference including figures). In addition, biologically active agents can also include but are not limited to anti-obesity related products, insulin, gastrin, prolactin, adrenocorticotrophic hormone (ACTH), thyroid stimulating hormone (TSH), luteinizing hormone (LH), follicle stimulating hormone

(FSH), human chorionic gonadotropin (HCG), motilin, interferons (alpha, beta, gamma), interleukins (IL-1 to IL-12), tumor necrosis factor (TNF), tumor necrosis factor-binding protein (TNF-bp), brain derived neurotrophic factor (BDNF), glial derived neurotrophic factor (GDNF), neurotrophic factor 3 (NT3), fibroblast growth factors (FGF), neurotrophic growth factor (NGF), bone growth factors such as osteoprotegerin (OPG), insulin-like growth factors (IGFs), macrophage colony stimulating factor (M-CSF), granulocyte macrophage colony stimulating factor (GM-CSF), megakaryocyte derived growth factor (MGDF), thrombopoietin, platelet-derived growth factor (PDGF), colony stimulating growth factors (CSFs), bone morphogenetic protein (BMP), superoxide dismutase (SOD), tissue plasminogen activator (TPA), urokinase, streptokinase and kallikrein. The term proteins, as used herein, includes peptides, polypeptides, consensus molecules, analogs, derivatives or combinations thereof.

Derivatives of biologically active agents may include the attachment of one or more chemical moieties to the protein moiety. Chemical modification of biologically active agents has been found to provide additional advantages under certain circumstances, such as increasing the stability and circulation time of the therapeutic protein and decreasing immunogenicity. One skilled in the art will be able to select the desired chemical modification based on the desired dosage, circulation time, resistance to proteolysis, therapeutic uses and other considerations.

As used herein, biodegradability refers to the breakdown of the molecular weight of a particular polymer into a smaller number of units in the chain, i.e., breakdown into lower molecular weight units. Biodegradable gel refers to the dissipation of the gel in the environment of use, where the dissipation is

contingent on the breakdown of the molecular weight of the constituent polymers, resulting in fewer units in the polymer chain.

5 Complexes

 The proteins, analog or derivative may be administered complexed to a binding composition. Such binding composition may have the effect of prolonging the circulation time of the protein, analog or
10 derivative or enhancing the activity of the biologically active agent. Such composition may be a protein (or synonymously, peptide), derivative, analog or combination. For example, a binding protein for the OB protein is OB protein receptor or portion thereof,
15 such as a soluble portion thereof. Other binding proteins may be ascertained by examining OB protein, or the protein of choice, in serum, or be empirically screening for the presence of binding. Such binding will typically not interfere with the ability of OB
20 protein or analog or derivative to bind to endogenous OB protein receptor and/or effect signal transduction. In addition to the OB protein, binding complexes will also be applicable to other therapeutic proteins of the present invention as well. Those well skilled in the
25 art will be able to ascertain appropriate binding proteins for use with the present invention.

 Likewise, precipitating agents used to precipitate the biologically active agent can be obtained from various commercial, natural or synthetic
30 sources which are well known in the art. Precipitating agents include but are not limited to polyvalent metal ions or their salts such as acetates, citrates, chlorides, carbonates, hydroxides, oxalates, tartrates or hydroxides thereof, acids or water soluble polymers.
35 In particular, the metal ions can include but are not limited to aluminum, barium, calcium, iron, manganese

magnesium, strontium and zinc. Preferably the metal ion is zinc or the salts thereof, like acetate chloride salts. Water soluble small molecules and salts can also be used such as ammonium sulfate, acetone, ethanol
5 and glycerol.

As for water soluble polymers these include but are not limited to polyethylene glycol, ethylene glycol/propylene glycol copolymers, carboxymethylcellulose, dextran, polyvinyl alcohol,
10 polyvinyl pyrrolidone, poly-1, 3-dioxolane, poly-1,3,6-trioxane, ethylene/maleic anhydride copolymers, polyaminoacids, dextran, poly (n-vinyl pyrrolidone) polyethylene glycol, propylene glycol homopolymers, polypropylene oxide/ethylene oxide
15 copolymers, polyoxyethylated polyols, polyvinyl alcohol succinate, glycerine, ethylene oxides, propylene oxides, poloxamers, alkoxyated copolymers, water soluble polyanions, derivatives or combinations thereof. The water soluble polymer may be of any
20 molecular weight, and may be branched or unbranched. For example, the preferred molecular weight of polyethylene glycol is between about 700 Da and about 100 kDa for ease in handling and efficiency of precipitation.

25 Other sizes and types of precipitating agents, may be used, depending on the desired therapeutic profile (e.g., the duration of sustained-release desired, the effects, if any on biological activity, the ease in handling, the degree or lack of
30 antigenicity and other known effects of a desired precipitating agent to a therapeutic protein or analog). One skilled in the art will appreciate other precipitating agents that are within the scope of the invention.

35 In addition, the compositions of the present invention may also include extra excipients necessary

to stabilize the biologically active agent and/or the hydrophilic polymer. These can be contained in the buffer and may include but are not limited to preservatives.

5

Pharmaceutical Compositions

The sustained-release pharmaceutical compositions of the present invention may be administered by oral (e.g., capsules such as hard capsules and soft capsules, solid preparations such as granules, tablets, pills, troches or lozenges, cachets, pellets, powder and lyophilized forms, liquid preparations such as suspensions) and non-oral preparations (e.g., intramuscular, subcutaneous, transdermal, visceral, IV (intravenous), IP (intraperitoneal), intraarterial, intrathecal, intracapsular, intraorbital, injectable, pulmonary, nasal, rectal, and uterine-transmucosal preparations).

In general, comprehended by the invention are sustained-release pharmaceutical compositions comprising effective amounts of protein, or derivative products, with the sustained-release compositions of the invention together with pharmaceutically acceptable diluents, preservatives, solubilizers, emulsifiers, adjuvants and/or carriers needed for administration. See PCT 97/01331 hereby incorporated by reference. The optimal pharmaceutical formulation for a desired biologically active agent will be determined by one skilled in the art depending upon the route of administration and desired dosage. Exemplary pharmaceutical compositions are disclosed in Remington's Pharmaceutical Sciences (Mack Publishing Co., 18th Ed., Easton, PA, pgs. 1435-1712 (1990)).

Due to the thixotropic nature of the delayed gel formulation, syringes can be used to administer subcutaneously. The composition may be gelled in a

syringe for later injection. This gelation can be performed in a time-delayed manner. The timing is controlled by the judicious adjustment of the quantity of the gelling agent and the proton donor in the mixture, if needed. Such a preparation would be used for later re-gelation in the body after injection. The term thixotropic as used herein refers to the viscosity of the gel mixture which decreases under pressure, e.g., from the syringe plunger, at which point the mixture can flow, e.g., through the syringe needle, and then reform a gel at the injection site.

The concept of delayed gelation can also be applied to filling a syringe where a sustained-release gel composition is filled in a syringe and at a preset time gels in the syringe, e.g., from a few minutes to many hours after filling. This avoids the problem of filling a syringe with material that has already gelled. These prefilled syringes can be stored for later injection into patients.

Components that may be needed for administration include diluents of various buffer content (e.g., Tris-HCl, acetate), pH and ionic strength; additives such as surfactants and solubilizing agents (e.g., Tween 80, HCO-60, Polysorbate 80), anti-oxidants (e.g., ascorbic acid, glutathione, sodium metabisulfite), additional polysaccharides (e.g., carboxymethylcellulose, sodium alginate, sodium hyaluronate, protamine sulfate, polyethylene glycol), preservatives (e.g., Thimersol, benzyl alcohol, methyl paraben, propyl paraben) and building substances (e.g., lactose, mannitol); incorporation of the material into particulate preparations of polymeric compounds such as polylactic/polyglycolic acid polymers or copolymers, etc. or combined with liposomes. Hylauronic acid may also be used as an administration component and this

may have the effect of promoting even further the sustained duration in the circulation. Additionally, sustained-release compositions of the present invention may also be dispersed with oils (e.g., sesame oil, corn oil, vegetable), or a mixture thereof with a phospholipid (e.g., lecitin), or medium chain fatty acid triglycerides (e.g., Miglyol 812) to provide an oily suspension. The compositions of the present invention may also be dispersed with dispersing agents such as water-soluble polysaccharides (e.g., mannitol, lactose, glucose, starches), hyaluronic acid, glycine, fibrin, collagen and inorganic salts (e.g., sodium chloride).

In addition, also contemplated for use in the administration of the sustained-release compositions of the present invention are mechanical devices designed for pulmonary delivery of therapeutic products, including but not limited to nebulizers, metered dose inhalers, and powder inhalers, all of which are familiar to those skilled in the art.

The administration components may influence the physical state, stability, rate of in vivo release, and rate of in vivo clearance of the present proteins and derivatives. One skilled in the art will appreciate the appropriate administration components and/or the appropriate mechanical devices to use depending on the therapeutic use, route of administration, desired dosage, circulation time, resistance to proteolysis, protein stability and other considerations.

Methods of Use

Therapeutic. Therapeutic uses depend on the biologically active agent used. One skilled in the art will readily be able to adapt a desired biologically active agent to the present invention for its intended

therapeutic uses. Therapeutic uses for such agents are set forth in greater detail in the following publications hereby incorporated by reference including drawings. Therapeutic uses include but are not limited to uses for proteins like interferons (see, U.S. Patent Nos. 5,372,808, 5,541,293 4,897,471, and 4,695,623 hereby incorporated by reference including drawings), interleukins (see, U.S. Patent No. 5,075,222, hereby incorporated by reference including drawings), erythropoietins (see, U.S. Patent Nos. 4,703,008, 5,441,868, 5,618,698 5,547,933, and 5,621,080 hereby incorporated by reference including drawings), granulocyte-colony stimulating factors (see, U.S. Patent Nos. 4,999,291, 5,581,476, 5,582,823, 4,810,643 and PCT Publication No. 94/17185, hereby incorporated by reference including drawings), stem cell factor (PCT Publication Nos. 91/05795, 92/17505 and 95/17206, hereby incorporated by reference including drawings), and the OB protein (see PCT publication Nos. 96/40912, 96/05309, 97/00128, 97/01010 and 97/06816 hereby incorporated by reference including figures).

In addition, therapeutic uses of the present invention include uses of biologically active agents including but not limited to anti-obesity related products, insulin, gastrin, prolactin, adrenocorticotrophic hormone (ACTH), thyroid stimulating hormone (TSH), luteinizing hormone (LH), follicle stimulating hormone (FSH), human chorionic gonadotropin (HCG), motilin, interferons (alpha, beta, gamma), interleukins (IL-1 to IL-12), tumor necrosis factor (TNF), tumor necrosis factor-binding protein (TNF-bp), brain derived neurotrophic factor (BDNF), glial derived neurotrophic factor (GDNF), neurotrophic factor 3 (NT3), fibroblast growth factors (FGF), neurotrophic growth factor (NGF), bone growth factors such as osteoprotegerin (OPG), insulin-like growth factors

(IGFs), macrophage colony stimulating factor (M-CSF), granulocyte macrophage colony stimulating factor (GM-CSF), megakaryocyte derived growth factor (MGDF), thrombopoietin, platelet-derived growth factor (PDGF),
5 colony stimulating growth factors (CSFs), bone morphogenetic protein (BMP), superoxide dismutase (SOD), tissue plasminogen activator (TPA), urokinase, streptokinase and kallikrein. The term proteins, as used herein, includes peptides, polypeptides, consensus
10 molecules, analogs, derivatives or combinations thereof. In addition, the present compositions may also be used for manufacture of one or more medicaments for treatment or amelioration of the conditions the biologically active agent is intended to treat.

15 By way of example, therapeutic uses (e.g., increase in blood oxygenation in the blood) and a decrease in bone resorption or osteoporosis may also be achieved in the absence of weight loss.

20 Combination Therapies. The present compositions and methods may be used in conjunction with other therapies, such as altered diet and exercise. Other medicaments, such as those useful for the treatment of diabetes (e.g., insulin, and possibly
25 amylin), cholesterol and blood pressure lowering medicaments (such as those which reduce blood lipid levels or other cardiovascular medicaments), activity increasing medicaments (e.g., amphetamines), diuretics (for liquid elimination), and appetite suppressants.
30 Such administration may be simultaneous or may be in seriatim. In addition, the present methods may be used in conjunction with surgical procedures, such as cosmetic surgeries designed to alter the overall appearance of a body (e.g., liposuction or laser
35 surgeries designed to reduce body mass, or implant surgeries designed to increase the appearance of body

mass). The health benefits of cardiac surgeries, such as bypass surgeries or other surgeries designed to relieve a deleterious condition caused by blockage of blood vessels by fatty deposits, such as arterial
5 plaque, may be increased with concomitant use of the present compositions and methods. Methods to eliminate gall stones, such as ultrasonic or laser methods, may also be used either prior to, during or after a course of the present therapeutic methods. Furthermore, the
10 present methods may be used as an adjunct to surgeries or therapies for broken bones, damaged muscle, or other therapies which would be improved by an increase in lean tissue mass.

15 Dosages

One skilled in the art will be able to ascertain effective dosages by administration and observing the desired therapeutic effect. The dosage of the sustained-release preparation is the amount
20 necessary to achieve the effective concentration of the biologically active agent in vivo, for a given period of time. The dosage and the preferred administration frequency of the sustained-release preparations varies with the type of the biologically active agent, the
25 desired duration of the release, the target disease, desired administration frequency, the subject animal species and other factors. Preferable, the formulation of the molecule will be such that between about 0.10 µg/kg/day and 100 mg/kg/day will yield the desired
30 therapeutic effect.

The effective dosages may be determined using diagnostic tools over time. By way of example, the present invention provides the dosages of OB protein. For example, a diagnostic for measuring the amount of
35 OB protein in the blood (or plasma or serum) may first

be used to determine endogenous levels of OB protein. Such diagnostic tool may be in the form of an antibody assay, such as an antibody sandwich assay. The amount of endogenous OB protein is quantified initially, and a
5 baseline is determined. The therapeutic dosages are determined as the quantification of endogenous and exogenous OB protein (that is, protein, analog or derivative found within the body, either self-produced or administered) is continued over the course of
10 therapy. For example, a relatively high dosage may be needed initially, until therapeutic benefit is seen, and then lower dosages used to maintain the therapeutic benefits.

15 Materials and Methods

Materials. Alginate in the form of sodium alginate can be found from sources well known in the art. OB protein and GCSF are from Amgen Inc. Other
20 chemicals are from sources well known in the art.

Alginate Hydrogel Particle/Bead Preparation. The preparation of the alginate hydrogel particles and beads, with and without proteins, is described in
25 detail in co-pending U.S. application 08/842,756, hereby incorporated by reference.

Delayed Gel Preparation. The preparation of the delayed alginate hydrogels, with and without
30 proteins, is described in detail in copending U.S. applications 08/857,913 and 08/912,902, each of which is hereby incorporated by reference.

The following examples are offered to more
35 fully illustrate the invention, but are not to be construed as limiting the scope thereof. In addition,

with respects to the above disclosure or the examples below, one skilled in the art will be able to make the necessary changes to the disclosures for large scale production.

5

EXAMPLE 1

The following example describes the preparation of alginate esters to be used in the present invention.

10

Preparation A : Tetrabutylammonium(TBA) alginate

A sulfonic acid resin (Bio-Rad, AG MP-50) is converted to the tetrabutylammonium(TBA) form by treatment with tetrabutylammonium hydroxide (Aldrich) using a batch method at room temperature. To a solution of 10 g of sodium salt of alginic acid in 800 ml of distilled water is added 60 ml of sulfonic resin (Bio-Rad, AG MP-50) in the tetrabutylammonium salt form. The mixture is stirred at room temperature for 0.5 hours. The resin is removed by filtration and washed with distilled water. The TBA alginate in the filtrate is isolated by freeze-drying (yield, 16.8 g) and confirmed by ^1H NMR.

25 Preparation B: Partial ethyl ester of alginic acid, degree of esterification (DE) = 30 mol%.

TBA alginate(6 g, 14.4mmol TBA units) is dissolved in 500 ml dimethyl sulfoxide (DMSO) at room temperature. Iodoethane (Aldrich, 673 mg, 4.3mmol) is then added. The mixture is stirred at 30°C for 15 hours, then cooled to room temperature. To this solution is slowly added a solution of 2 g NaCl in 20 mL water to completely convert the TBA to the sodium salt. After stirring 15-30 min, the solution is slowly poured into 1500 mL ethyl acetate. The precipitate is

collected by filtration and washed three times with acetone/water (8:1 v/v) and three times with acetone, then vacuum dried. The compound is redissolved in distilled water (~100 mL) and the pH adjusted to ~6.5
5 with 0.2% NaHCO₃ at 0°C. The solution is then dialyzed (MW cut-off 8000) overnight against distilled water at 4°C and then freeze-dried. The yield of the partial ester is 2.8 g and the degree of esterification is 30 +/- 1% (¹H NMR, maleimide as internal standard).

10

Preparation C: Total and partial ethyl ester of alginic acid, DE = 100%, 50%, 20%, 10% and 5%.

The preparation of these compounds is similar to that described in Preparation B except that the
15 amount of iodoethane added is adjusted to arrive at the desired degree of esterification.

Preparation D: Partial propyl, hexyl, octyl and dodecyl esters of alginic acid.

20 The preparations are similar to that described in Preparations B and C above, but substituting 1-iodopropane, 1-iodohexane, 1-iodooctane or 1-iodododecane for iodoethane respectively.

25 Preparation E: Partial benzyl ester of alginic acid, DE = 30%.

TBA alginate (2.5 g, 5.99 mmol TBA units) is dissolved in ~200 mL DMSO at room temperature. Benzyl bromide (Aldrich, 307 mg, 1.8 mmol) and TBA iodide
30 (Aldrich, 30 mg) are added. The mixture is stirred at 30°C for 15 hours, and then cooled to room temperature. To this solution is slowly added a solution of 0.6 g NaCl in 10 mL water to completely convert the TBA to the sodium salt. After stirring 15-30 minutes, the
35 solution is slowly poured into 500 mL ethyl acetate.

- 29 -

The precipitate is collected by filtration and washed three times with acetone/water (8:1 v/v) and three times with acetone, then vacuum dried. The compound is redissolved in distilled water (~60 mL) and adjusted to
5 pH ~6.5 with 0.2% NaHCO₃ at 0°C, then dialyzed (MW cut-off 8000) overnight against distilled water at 4°C. The yield of the partial ester is 1.3 g and the degree of esterification is 30 +/- 1% (¹H NMR, maleimide as internal standard).

10

Preparation F: Total and partial benzyl ester of alginic acid with different DE.

The preparation of these compounds is similar to that described in Preparation E except that the
15 amount of benzyl bromide and TBA iodide added are adjusted to arrive at the desired degree of esterification.

EXAMPLE 2

20 The following example shows the preparation of a protein drug(Leptin)-containing alginate ethyl ester (DE = 15 mol% and 10 mol%) gel and the in vitro sustained release from this gel.

Leptin (100mg/mL; 10mM Tris HCl, pH 8.8; pH
25 adjusted from 8.0 to 8.8 with 1M NaOH) and 6% ethyl ester alginate (15 mol%, 10mM Tris HCl, pH 8.6) are cooled on an ice bath. Leptin (0.5 mL) is added to the 6% ethyl ester alginate (0.18 mL) and the mixture stirred on an ice bath for 10-15 min; the final pH is
30 8.6-8.8. To this mixture is added a suspension of 1M CaCO₃ (16 µL) and the resulting suspension is mixed well. To this suspension is dropwise added, with stirring, a solution of 0.1M ZnCl₂ (100 µL); water is then added to bring the volume to 1 mL. The mixture is

- 30 -

mixed completely and kept on an ice bath for 10-20 min. Then a solution of 1.68M δ -gluconolactone (Aldrich, 56 μ L) is thoroughly stirred into this mixture. The final mixture (50 mg/mL leptin, 1% ethyl ester alginate; 0.1 mL) is cast on the inside of an eppendorf tube and left overnight at 4°C to gel. After overnight storage, in vitro release is conducted in 10mM histidine buffer, pH 7.4. The cast gel with 15 mol% degree of esterification exhibits minimal burst and fairly constant leptin release showing 60% released in 6 days. The cast gel with 10 mol% degree of esterification exhibits minimal burst and fairly constant leptin release showing 55% released in 6 days.

15

EXAMPLE 3

20

The following example shows the preparation of a protein drug (Leptin)-containing alginate hexyl ester (DE = 15 mol% and 10 mol%) gel and the in vitro sustained release from this gel.

25

This example is performed in a similar manner as that described in Example 2 except that the ethyl ester alginate

30

The hexyl ester alginate gels with 15 mol% and 10 mol% of degree of esterification exhibit minimal burst and exhibits sustained release showing 50% released in 6 days.

EXAMPLE 4

The following example shows the preparation of a protein drug (Zn-Leptin)-containing alginate ethyl ester (DE = 15 mol%) gel and the in vitro sustained release from this gel.

5 To a solution of 4%(w/v) ethyl ester alginate (15 mol%, 0.75 mL) is added 1M Tris HCl pH 8.0 (7.5 μ L), 0.5 M PIPES pH 6.8 (33 μ L) and 0.1 M ZnCl_2 (8.5 μ L). The mixture is stirred well. To this solution is added Zn-leptin suspension (100 mg/mL, 10 675 μ L) and the mixture thoroughly stirred. A suspension of 1M CaCO_3 (24 μ L) and a solution of 1.68M d-gluconolactone (70 μ L) are then thoroughly stirred into this mixture. The final mixture (0.1 mL) is cast on the inside of an eppendorf tube and left overnight 15 at 4°C to gel. After overnight storage in vitro release is conducted in 10mM histidine buffer, pH 7.4. This cast ethyl ester alginate gel with 15 mol% degree of esterification exhibits little burst and sustained leptin release showing 65% released in 4 days.

20

EXAMPLE 5

The following example shows the preparation of a protein drug(GCSF)-containing alginate ethyl ester (DE = 30 mol%) gel and the in vitro sustained release 25 from this gel.

To a solution of 2.39% ethyl ester alginate (30 mol%, 0.50mL) is added 0.1M acetate buffer (pH 4.5, 100 μ L), GCSF (104 μ L, 48.2 mg/mL, HCl pH3) and distilled water (246 mL). The mixture is stirred well. 30 A suspension of 1M CaHPO_4 (10 μ L) and a solution of 1.68M δ -gluconolactone (40 μ L) are thoroughly stirred into this mixture. The final mixture (0.2 mL) is cast on the inside of an eppendorf tube and left overnight

at 4°C to gel. After overnight storage of the gel in vitro release is conducted in 10mM Tris buffer, pH 7.5. This cast ethyl ester alginate gel with 30 mol% degree of esterification exhibits less than 5% burst and
5 sustained release showing 20% released in 1 day and 40% released in 2 days.

EXAMPLE 6

10 The following example shows the preparation of a protein drug (GCSF)-containing alginate benzyl ester (DE = 30 mol%) gel and the in vitro sustained release from this gel.

This example is performed in a similar manner
15 that described in Example 5 except the ethyl ester is replaced by the benzyl ester alginate. The ester alginate gels within the overnight storage period. The benzyl ester alginate gel with 30% of degree of esterification exhibits less 5% burst and sustained
20 release showing 40% released in 1 day and 80% released in 2 days.

EXAMPLE 7

This example shows the preparation of
25 alginate ethyl ester beads.

The gel beads are prepared by adding dropwise a 2% ester alginate solutions into 100mM calcium chloride solutions (distilled water or 1M Tris HCl pH 7.0 buffer). The formed beads are washed with
30 distilled water or buffer. Beads are prepared using either 30% or 50% degree of esterification.

EXAMPLE 8

This example shows the preparation of Leptin-containing alginate ester beads.

The beads are prepared by adding dropwise a solution of 25 mg/mL Leptin in 2% ethyl ester alginate (Tris HCl, pH 8.7) into a solution of 100mM calcium chloride and 25mM zinc chloride. The beads are prepared using 30% degree of esterification. The beads demonstrate sustained leptin release in vitro.

10

EXAMPLE 9

This example shows the molecular weight breakdown (or degradation) of ester alginates in buffers at neutral physiological pH.

15

Alginate esters (1% solution) are dissolved in either phosphate buffer (0.1M sodium phosphate, pH 6.8) or 0.1M Tris buffer (pH 7.0) and incubated at 37°C. The molecular weight breakdown is determined by measuring the decrease in the solution viscosity

20

(Brookfield, 25°C) at selected time intervals.

25

Unmodified sodium alginate is found to be relatively stable in that its viscosity decreased only 5% in 8 days (phosphate buffer); however with ethyl and benzyl esters of alginic acid (DE = 30%) the viscosity drops 35% in 8 days in same buffer. The amount of degradation of esters of alginic acid is also dependent on the degree of esterification, e.g., with ethyl ester of lower degree of esterification (DE = 15%) the viscosity decreases 25% in 8 days. Thus the molecular weight breakdown is directly related to the degree of esterification.

30

EXAMPLE 10

This example shows the in vivo degradation (or gradual disappearance) of alginate ester hydrogels without protein and hydrogels containing protein.

The ester alginate gels are prepared in a similar manner to that described in Example 3 but the final mixture is taken up in a syringe and allowed to gel in the syringe at 4°C overnight. Then 100 µL of gel is injected subcutaneously into the back of the neck of mice (Charles River, 12 week old female, BDF1, 20 g, 5 mice per group) and the site surgically examined periodically on different members of the group.

Using ethyl and benzyl ester alginate material with DE = 30%, the results of the single injection site study show that the ester alginate hydrogels disappear within 2 weeks. Using ethyl ester alginate gel with DE = 15%, the gels are still present at 30 and 61 days, but reduced in size. Using ethyl ester alginate material with DE = 5%, the gels are still present at 30 and 61 days with little reduction in size. Using the unsubstituted sodium alginate material, the gel persists relatively unchanged through day 61.

The rate of disappearance of the ester alginate gels is similar with or without protein.

EXAMPLE 11

This example provides weight loss and pharmacokinetics data for leptin-containing alginate ester hydrogels in rats.

The ethyl ester alginate gels are prepared in a similar manner to that described in Example 4 but the final mixture is taken up in a syringe and allowed to gel in the syringe at 4°C overnight. Rats are given a

bolus dose of 0 mg/kg (control) and 100 mg/kg, then blood levels and weight loss are monitored for seven days.

The results show: the ethyl ester alginate with DE = 5 mol% exhibits a steady blood level of ~2000 ng/mL for 3 days, then declines to 2 ~ 3 ng/mL over the next 3-4 days; the ethyl ester alginate with DE = 15 mol% exhibits a steady blood level of ~ 2000 ng/mL for 2 days, then declines to 2-3 ng/mL at 5 days; the ethyl ester alginate with DE = 30 mol% exhibits a blood level of ~2000 ng/mL for 1 day, which decreases to 2-3 ng/mL at 4 days; the blood level of Zn-leptin suspension peaks at 12 hr, then decreases to 1-2 ng/mL at 6 days. All animals exhibit weight loss showing that the Zn-leptin is active. The results also show that incorporating Zn-leptin in the ethyl ester alginate gels (DE = 5 mol% and 15 mol%) nearly doubles (factor of 1.8 - 1.9) the area under the curve (AUC) of the Zn-leptin, suggesting a doubling of the bioavailability; and use of ethyl ester alginate gel (DE = 30 mol%) shows a similar bioavailability to Zn-leptin, based on AUC.

CLAIMS

We Claim:

- 5 1. A sustained-release delayed gel composition, comprising:
- a) a hydrophilic polymer;
 - b) a biologically active agent; and
 - c) at least one bound polyvalent metal
- 10 ion, wherein said gel is biodegradable.
2. The sustained-release composition of Claim 1 wherein the bound polyvalent metal ion is a mixture of bound and unbound polyvalent metal ion.
- 15 3. The sustained-release delayed gel of claim 1 further comprising excipients for stabilizing the biologically active agent or the hydrophilic polymer.
- 20 4. The composition of Claim 1 wherein the bound polyvalent metal ion is a salt selected from the group consisting of acetates, phosphates, lactates, tartrates, citrates, chlorides, carbonates or
- 25 hydroxides thereof.
5. The composition of Claim 4 wherein the metal ion is selected from the group consisting of manganese, strontium, iron, magnesium, calcium, barium,
- 30 copper, aluminum or zinc.
6. The composition of Claim 5 wherein the metal ion is calcium.
- 35 7. The composition of Claim 1 wherein the proton donor is from an acid source.

8. The composition of Claim 7 wherein the acid source is selected from the group consisting of buffers, esters, slowly dissolving acids or lactones.

5

9. The composition of Claim 1 wherein the hydrophilic polymer is a polyanion.

10. The composition of Claim 1 wherein the hydrophilic polymer is a polysaccharide.

10

11. The composition of Claim 10 wherein the polysaccharide is an acidic polysaccharide.

15

12. The composition of Claim 11 wherein the polysaccharide is alginate.

13. The composition of Claim 12 wherein the alginate contains at least 30% guluronic acid.

20

14. The composition of Claim 12 wherein the alginate consist of at least 0.05% by weight.

15. The composition of Claim 1 wherein the biologically active agent comprises a protein, and wherein the composition demonstrates improved bioavailability.

25

16. The composition of Claim 15 wherein the protein consist of at least 0.001 mg/ml.

30

17. The composition of Claim 15 wherein the protein is selected from the group consisting of hematopoietic factors, colony stimulating factors, anti-obesity factors, growth factors, trophic factors, and antiinflammatory factors.

35

18. The composition of Claim 15 wherein the protein is selected from the group consisting of leptin, G-CSF, SCF, BDNF, GDNF, NT3, GM-CSF, IL-1ra,
5 IL2, TNF-bp, MGDF, OPG, interferons, erythropoietin, KGF, insulin and analogs or derivatives thereof.

19. The composition of Claim 1 wherein the biologically active agent is a complexed biologically
10 active agent.

20. The composition of Claim 19 wherein the complexed biologically active agent is a precipitated protein.
15

21. The composition of Claim 20 wherein the precipitated protein is a zinc leptin precipitate.

22. A method of producing a sustained-
20 release delayed gel composition, wherein said gel is biodegradable, comprising the steps of:

a) mixing a biologically active agent and a hydrophilic polymer in a solvent to form a first mixture;
25

b) mixing to the first mixture at least one bound polyvalent metal ion to form a second mixture.

23. A method of Claim 22 further comprising
30 the step of c) mixing to the second mixture at least one proton donor capable of releasing the bound polyvalent metal ion.

24. The method of Claims 22 wherein the
35 first mixture is concentrated before mixing the proton donor or bound polyvalent metal ion.

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25. The method of Claim 22 wherein the bound polyvalent metal ion is a salt selected from the group consisting of acetates, phosphates, lactates, citrates,
5 tartrates, chlorides, carbonates or hydroxides thereof.

26. The method of Claim 22, wherein said method provides for a substantially constant blood level of said biologically active agent over time in
10 the patient.

27. The composition of Claim 24 wherein the metal ion is selected from the group consisting of manganese, strontium, iron, magnesium, calcium, barium,
15 copper, aluminum or zinc.

28. The composition of Claim 26 wherein the metal ion is calcium.

29. The composition of Claim 23 wherein the proton donor is from an acid source.

30. The composition of Claim 28 wherein the slow dissolving acid is selected from the group
25 consisting of buffers, esters, slowly dissolving acids or lactones.

31. The composition of Claim 29 wherein the acid source is δ -gluconolactone.
30

32. The composition of Claim 22 wherein the hydrophilic polymer is a polyanion.

33. The composition of Claim 22 wherein the
35 hydrophilic polymer is a polysaccharide.

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34. The composition of Claim 32 wherein the polysaccharide is an acidic polysaccharide.

35. The composition of Claim 33 wherein the
5 polysaccharide is alginate.

36. The composition of Claim 34 wherein the alginate contains at least 30% guluronic acid.

10 37. The composition of Claim 34 wherein the alginate consist of at least 0.05% by weight.

38. The composition of Claim 22 wherein the biologically active agent comprises a protein.
15

39. The composition of Claim 37 wherein the protein consist of at least 0.001 mg/ml.

40. The composition of Claim 37 wherein the
20 protein is selected from the group consisting of hematopoietic factors, colony stimulating factors, anti-obesity factors, growth factors, trophic factors, and antiinflammatory factors.

25 41. The composition of Claim 37 wherein the protein is selected from the group consisting of leptin, G-CSF, SCF, BDNF, GDNF, NT3, GM-CSF, IL-1ra, IL2, TNF-bp, MGDF, OPG, interferons, erythropoietin, KGF and analogs or derivatives thereof.

30 42. The composition of Claim 22 wherein the biologically active agent is a complexed biologically active agent.

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43. The composition of Claim 41 wherein the complexed biologically active agent is a precipitated protein.

5 44. The composition of Claim 42 wherein the precipitated protein is a zinc leptin precipitate.

45. The method of Claim 22 further comprising the step of isolating the sustained-release
10 composition.

46. The sustained-release product produced by the method of Claims 22 or 44.

15 47. A pharmaceutical formulation comprising the sustained-release composition according to Claims 1, 2, 3 or 45 in a pharmaceutically acceptable carrier, diluent or adjuvant.

20 48. The pharmaceutical formulation of Claim 46, wherein the formulation is in a syringe.

49. A method of treating an indication with a sustained-release composition according to Claims 1,
25 2, 3 or 45 in a pharmaceutically acceptable carrier, diluent or adjuvant.

50. A method of treatment of a disorder selected from the group consisting of excess weight,
30 diabetes, high blood lipid level, artherial sclerosis, artherial plaque, the reduction or prevention of gall stones formation, insufficient lean tissue mass, insufficient sensitivity to insulin, and stroke, with a sustained-release composition according to Claims 1, 2,
35 3, or 45 in a pharmaceutically acceptable carrier,

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diluent, or adjuvant wherein the biologically active agent is leptin, an analog or derivative thereof

51. A method of treating a disorder selected
5 from the group consisting of hematopoietic cell deficiencies, infection, and neutropenia with a sustained-release composition according to Claims 1, 2, 3, or 45 in a pharmaceutically acceptable carrier, diluent, or adjuvant wherein the biologically active
10 agent is G-CSF, an analog or derivative thereof.

52. A method of treating inflammation with a sustained-release composition according to Claims 1, 2, 3, or 45 in a pharmaceutically acceptable carrier,
15 diluent, or adjuvant, wherein the biologically active agent is an IL-1ra, an analog or derivative thereof.

53. A sustained-release composition,
comprising:
20 a) a hydrophilic polymer;
b) a biologically active agent; and
c) at least one precipitating agent;
characterized in that the biologically active agent is co-precipitated within the hydrophilic polymer, wherein
25 said composition is in the form of a gel particle, and wherein said particle is biodegradable.

54. The composition of Claim 52 wherein the precipitating agent is selected from the group
30 consisting of polyvalent metal ions or salts, acetates, citrates, chlorides, carbonates or hydroxides thereof.

55. The composition of Claim 53 wherein the metal ion is selected from the group consisting of
35 manganese, strontium, iron, magnesium, calcium, barium, aluminium or zinc.

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56. The composition of Claim 54 wherein the precipitating agent is a polyvalent ion selected from the group consisting of zinc, calcium or a combination thereof.

57. The composition of Claim 52 wherein the hydrophilic polymer is a polysaccharide.

58. The composition of Claim 56 wherein the polysaccharide is alginate.

59. A method of producing a sustained-release composition, comprising the steps of:

- a) dissolving a biologically active agent and a hydrophilic polymer with a solvent to form a first mixture;
- b) dissolving at least one precipitating agent in a solvent to form a second mixture;
- c) adding the first mixture with the second mixture; and
- d) co-precipitating the biologically active agent with the hydrophilic polymer to form a co-precipitated gel particle, wherein said particle is biodegradable.

60. The method of Claim 58 further comprising the step of isolating the co-precipitated particle.

61. The sustained-release product produced by the method of Claim 59.

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62. A pharmaceutical formulation according to Claims 52 in a pharmaceutically acceptable carrier, diluent or adjuvant.

5 63. A method of treating an indication with a sustained-release composition according to Claim 52 in a pharmaceutically acceptable carrier, diluent or adjuvant.

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INTERNATIONAL SEARCH REPORT

International Application No PCT/US 99/10737		
A. CLASSIFICATION OF SUBJECT MATTER IPC 6 A61K9/16 A61K47/36		
According to International Patent Classification (IPC) or to both national classification and IPC		
B. FIELDS SEARCHED Minimum documentation searched (classification system followed by classification symbols) IPC 6 A61K		
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched		
Electronic data base consulted during the international search (name of data base and, where practical, search terms used)		
C. DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
P, X	WO 98 51348 A (AMGEN INC ;GU JIAN HUA (US); BEEKMAN ALICE C (US); GOLDENBERG MERR) 19 November 1998 (1998-11-19) cited in the application the whole document ---	1-63
P, X	WO 98 46211 A (AMGEN INC) 22 October 1998 (1998-10-22) cited in the application the whole document ---	1-63
-/-		
<div style="display: flex; justify-content: space-between;"> <input checked="" type="checkbox"/> Further documents are listed in the continuation of box C. <input checked="" type="checkbox"/> Patent family members are listed in annex. </div>		
* Special categories of cited documents :		
<div style="display: flex;"> <div style="flex: 1;"> <p>"A" document defining the general state of the art which is not considered to be of particular relevance</p> <p>"E" earlier document but published on or after the international filing date</p> <p>"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>"O" document referring to an oral disclosure, use, exhibition or other means</p> <p>"P" document published prior to the international filing date but later than the priority date claimed</p> </div> <div style="flex: 1;"> <p>"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone</p> <p>"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.</p> <p>"&" document member of the same patent family</p> </div> </div>		
Date of the actual completion of the international search <div style="text-align: center; font-weight: bold;">26 August 1999</div>		Date of mailing of the international search report <div style="text-align: center; font-weight: bold;">10/09/1999</div>
Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Tx. 31 651 epo nl, Fax: (+31-70) 340-3016		Authorized officer <div style="text-align: center; font-weight: bold;">Boulois, D</div>

INTERNATIONAL SEARCH REPORT

International Application No

PCT/US 99/10737

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	<p>WO 96 00081 A (IMMUNEX CORP) 4 January 1996 (1996-01-04)</p> <p>page 6 - page 7; example 1 page 9; example 4</p> <p style="text-align: center;">---</p>	<p>1-18,22, 23, 25-30, 32-41, 45-49, 52-63</p>
X	<p>US 5 700 848 A (HEINTZ ROSWITHA A ET AL) 23 December 1997 (1997-12-23)</p> <p>column 8, line 12 - column 9, line 37 column 12; example 9 column 17 - column 18; examples 21,22 column 20; example 27</p> <p style="text-align: center;">---</p>	<p>1-3,5,6, 9-12,14, 15,17, 22,23, 26-28, 32-35, 37,38, 40,46, 47,53-63</p>
X	<p>PATENT ABSTRACTS OF JAPAN vol. 013, no. 174 (C-589), 25 April 1989 (1989-04-25) & JP 01 005460 A (SAN EI CHEM IND LTD), 10 January 1989 (1989-01-10)</p> <p style="text-align: center;">---</p>	<p>1-11,15, 22,23, 25-30, 34,38, 46,47, 49, 53-57, 59,62,63</p>
X	<p>abstract & DATABASE WPI Week 8907 Derwent Publications Ltd., London, GB; AN 89-049865 & JP 01 005460 A (SAN-EI CHEM IND LTD)</p> <p style="text-align: center;">---</p> <p>abstract</p>	<p>1-11,15, 22,23, 25-30, 34,38, 46,47, 49, 53-57, 59,62,63</p>
X	<p>EP 0 719 548 A (MCNEIL PPC INC) 3 July 1996 (1996-07-03)</p> <p>page 3, line 3 - line 5 page 4 - page 5; example 1 page 5 - page 7; examples 3,5</p> <p style="text-align: center;">---</p>	<p>1-8, 22-30, 46,47, 49,53-57</p>
X	<p>EP 0 613 693 A (JOHNSON & JOHNSON MEDICAL) 7 September 1994 (1994-09-07) page 3, line 32 - line 39 page 3, line 53 - line 58 page 4 - page 5; examples 2,3</p> <p style="text-align: center;">---</p>	<p>1-12,14, 46,47</p>
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INTERNATIONAL SEARCH REPORT

International Application No

PCT/US 99/10737

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	<p>TATESHITA, KENGO ET AL: "Preparation and evaluation of a controlled-release formulation of nifedipine using alginate gel beads"</p> <p>BIOL. PHARM. BULL. (1993), 16(4), 420-4 , XP002113458</p> <p>the whole document</p> <p>-----</p>	<p>1-14,</p> <p>22-30,</p> <p>32-37,</p> <p>46,47,</p> <p>49,53-63</p>

Form PCT/ISA/210 (continuation of second sheet) (July 1992)

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US 99/ 10737

Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☐ Claims Nos.:
because they relate to subject matter not required to be searched by this Authority, namely:
2. ☒ Claims Nos.: 1, 22, 53, 59
because they relate to parts of the International Application that do not comply with the prescribed requirements to such an extent that no meaningful International Search can be carried out, specifically:

see FURTHER INFORMATION sheet PCT/ISA/210
3. ☐ Claims Nos.:
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this International Search Report covers all searchable claims.
2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this International Search Report covers only those claims for which fees were paid, specifically claims Nos.:
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest.
- ☐ No protest accompanied the payment of additional search fees.

FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210

Continuation of Box I.2

Claims Nos.: 1,22,53,59

Present claims 1,22,53, and 59 relate to an extremely large number of possible compounds comprised by the terms "hydrophilic polymer", "biologically active agent" and "bound polyvalent metal ion".

Support within the meaning of Article 6 PCT and/or disclosure within the meaning of Article 5 PCT is to be found, however, for only a very small proportion of the compounds claimed. In the present case, the claims so lack support, and the application so lacks disclosure, that a meaningful search over the whole of the claimed scope is impossible. Consequently, the search has been carried out for those parts of the claims which appear to be supported and disclosed, namely those parts relating to the compounds which are claimed and disclosed in the examples of the present application.

The applicant's attention is drawn to the fact that claims relating to inventions in respect of which no international search report has been established need not be the subject of an international preliminary examination (Rule 66.1(e) PCT). The applicant is advised that the EPO policy when acting as an International Preliminary Examining Authority is normally not to carry out a preliminary examination on matter which has not been searched. This is the case irrespective of whether or not the claims are amended following receipt of the search report or during any Chapter II procedure.

INTERNATIONAL SEARCH REPORT

Information on patent family members

1. national Application No

PCT/US 99/10737

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
WO 9851348 A	19-11-1998	AU 7491898 A	08-12-1998
WO 9846211 A	22-10-1998	AU 6973498 A ZA 9803089 A	11-11-1998 19-10-1998
WO 9600081 A	04-01-1996	AU 698393 B AU 2870995 A EP 0766564 A JP 10503179 T NZ 288997 A	29-10-1998 19-01-1996 09-04-1997 24-03-1998 28-01-1999
US 5700848 A	23-12-1997	US 5837747 A US 5846530 A US 5705270 A AU 3124793 A CA 2121129 A EP 0610441 A JP 7503943 T WO 9309176 A	17-11-1998 08-12-1998 06-01-1998 07-06-1993 13-05-1993 17-08-1994 27-04-1995 13-05-1998
JP 01005460 A	10-01-1989	NONE	
EP 0719548 A	03-07-1996	US 5660859 A AU 692959 B AU 4050295 A DE 69509055 D DE 69509055 T JP 8253412 A NZ 280609 A US 5840337 A	26-08-1997 18-06-1998 04-07-1996 20-05-1999 19-08-1999 01-10-1996 24-11-1997 24-11-1998
EP 0613693 A	07-09-1994	GB 2275686 A AT 174802 T AU 676706 B AU 5755694 A CA 2116743 A DE 69415366 D DE 69415366 T ES 2126060 T JP 6343684 A ZA 9401343 A	07-09-1994 15-01-1999 20-03-1997 08-09-1994 04-09-1994 04-02-1999 17-06-1999 16-03-1999 20-12-1994 25-08-1995